

(12) INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(19) World Intellectual Property Organization  
International Bureau



(43) International Publication Date  
18 July 2002 (18.07.2002)

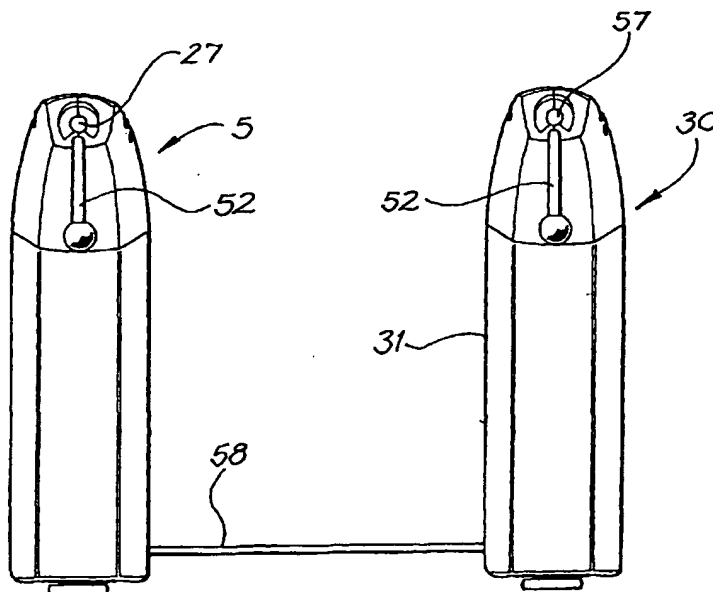
PCT

(10) International Publication Number  
**WO 02/056637 A1**

- (51) International Patent Classification<sup>7</sup>: **H04R 25/00**, A61N 1/36 (74) Agent: **F B RICE & CO**; 605 Darling Street, Balmain, NSW 2041 (AU).
- (21) International Application Number: **PCT/AU02/00036** (81) Designated States (*national*): AE, AG, AL, AM, AT, AU, AZ, BA, BB, BG, BR, BY, BZ, CA, CH, CN, CO, CR, CU, CZ, DE, DK, DM, DZ, EC, EE, ES, FI, GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MA, MD, MG, MK, MN, MW, MX, MZ, NO, NZ, OM, PH, PL, PT, RO, RU, SD, SE, SG, SI, SK, SL, TJ, TM, TN, TR, TT, TZ, UA, UG, US, UZ, VN, YU, ZA, ZM, ZW.
- (22) International Filing Date: 14 January 2002 (14.01.2002)
- (25) Filing Language: English
- (26) Publication Language: English
- (30) Priority Data: PR 2504 12 January 2001 (12.01.2001) AU (84) Designated States (*regional*): ARIPO patent (GH, GM, KE, LS, MW, MZ, SD, SL, SZ, TZ, UG, ZM, ZW), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE, TR), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, GQ, GW, ML, MR, NE, SN, TD, TG).
- (71) Applicant (*for all designated States except US*): **COCHLEAR LIMITED** [AU/AU]; 14 Mars Road, Lane Cove, NSW 2066 (AU).
- (72) Inventor; and
- (75) Inventor/Applicant (*for US only*): **SELIGMAN, Peter** [AU/AU]; 107 Fawkner Street, Essendon, VIC 3040 (AU). Published: — with international search report

[Continued on next page]

(54) Title: "GENERAL PURPOSE ACCESSORY FOR A COCHLEAR IMPLANT SYSTEM"



(57) Abstract: A cochlear implant system comprising a first unit (5) adapted to be worn on or in one ear of an implantee. The first unit has a case housing componentry including a microphone (27), and a speech processor means (29). A second unit or accessory (30) is adapted to be worn on or in the other ear of the implantee. The second unit or accessory (30) has a case (31) housing a second power source. An electrical conduction means (58) for transmitting power from the second power source to the componentry of the first unit extends between the first and second units. Such a conduction means (58) can extend around the back of the head of the implantee.

WO 02/056637 A1



*For two-letter codes and other abbreviations, refer to the "Guidance Notes on Codes and Abbreviations" appearing at the beginning of each regular issue of the PCT Gazette.*

## "General purpose accessory for a cochlear implant system"

### Field of the Invention

The present invention relates to an accessory for use with a cochlear  
5 implant system.

### Background of the Invention

In many people who are profoundly deaf, the reason for deafness is  
absence of, or destruction of, the hair cells in the cochlea which transduce  
10 acoustic data signals into nerve impulses. These people are thus unable to  
derive suitable benefit from conventional hearing aid systems, no matter how  
loud the acoustic stimulus is made, because there is damage to or absence of  
the mechanism for nerve impulses to be generated from sound in the normal  
manner.

15 It is for this purpose that cochlear implant systems have been  
developed. Such systems bypass the hair cells in the cochlea and directly  
deliver electrical stimulation to the auditory nerve fibres, thereby allowing  
the brain to perceive a hearing sensation resembling the natural hearing  
sensation normally delivered to the auditory nerve. US Patent 4532930, the  
20 contents of which are incorporated herein by reference, provides a  
description of one type of traditional cochlear implant system.

Typically, cochlear implant systems have consisted of essentially two  
components, an external component commonly referred to as a processor unit  
and an internal implanted component commonly referred to as a  
25 stimulator/receiver unit. Traditionally, both of these components have  
cooperated together to provide the sound sensation to an implantee.

The external component has traditionally consisted of a microphone  
for detecting sounds, such as speech and environmental sounds, a speech  
processor that converts the detected sounds, particularly speech, into a coded  
30 signal, a power source such as a battery, and an external transmitter coil.

The coded signal output by the speech processor is transmitted  
transcutaneously to the implanted stimulator/receiver unit situated within a  
recess of the temporal bone of the implantee. This transcutaneous  
transmission occurs via the external transmitter coil which is positioned to  
35 communicate with an implanted receiver coil provided with the  
stimulator/receiver unit. This communication serves two essential purposes,

firstly to transcutaneously transmit the coded sound signal and secondly to provide power to the implanted stimulator/receiver unit. Conventionally, this link has been in the form of a radio frequency (RF) link, but other such links have been proposed and implemented with varying degrees of success.

5       The implanted stimulator/receiver unit traditionally includes a receiver coil that receives the coded signal and power from the external processor component, and a stimulator that processes the coded signal and outputs a stimulation signal to an intracochlea electrode assembly which applies the electrical stimulation directly to the auditory nerve producing a hearing  
10 sensation corresponding to the original detected sound.

Traditionally, the external componentry has been carried on the body of the implantee, such as in a pocket of the implantee's clothing, a belt pouch or in a harness, while the microphone has been mounted on a clip mounted behind the ear or on the lapel of the implantee.

15       More recently, due in the main to improvements in technology, the physical dimensions of the speech processor have been able to be reduced allowing for the external componentry to be housed in a small unit capable of being worn behind the ear of the implantee. This unit allows the microphone, power unit and the speech processor to be housed in a single  
20 unit capable of being more discretely worn behind the ear, with the external transmitter coil still positioned on the side of the implantee's head to allow for the transmission of the coded sound signal from the speech processor and power to the implanted stimulator unit. The availability of such behind-the-ear (BTE) units has provided a great benefit to cochlear implant system  
25 recipients and provided them with a new found freedom. This has been due in the main to there no longer being a need to carry a large unit around with them and the associated long cables to connect the body worn device to the microphone and the transmitter coil positioned on the side of their head.

While the dimensions of behind-the-ear units have reduced  
30 significantly from those worn on the body, the units are typically still larger than most conventional hearing aids due in the main to the space requirements for the speech processor and batteries within this unit as well as the intrinsic differences between hearing aids and cochlear implant devices. As behind-the-ear units need to satisfy the power requirements of  
35 the implant, a large proportion of the size of conventional behind-the-ear devices has been associated with housing the power source (batteries) to

provide such power requirements. As the power requirements of implant recipients vary depending upon the coding strategies that are employed and the skin flap thickness of the recipient across which the power needs to be transmitted, a main design limitation of conventional behind-the-ear devices  
5 has resided in housing a sufficient power supply to cater for all recipient types.

While continuing improvements in microprocessor and battery design should lead to further miniaturisation of behind-the-ear units, perhaps to the extent that the unit could be worn within the ear, implantee expectations as  
10 to the level of performance and features of cochlear implant systems are also expected to increase. In order to meet this implantee expectation, it is anticipated that there would need to be an unacceptably large increase in the size of presently known behind the ear units so negating any efforts to further miniaturise such units in the future.

15 Further to this, in most cases of cochlear implantation, the implant has only been implanted in one of the patient's cochleas, with the decision upon which ear the implantation is to occur being the result of extensive pre-operative consideration. Due to the design requirements of the conventional system, the cochlear implant system user finds that if they desire to wear a  
20 behind-the-ear processor, then in most cases they will wear it on the ear that has been implanted in order to reduce the amount of connecting leads required. It has been accepted that in the majority of cases when the patient has been implanted in only one ear, that for simplicity of use, the behind-the-ear unit has been worn on the ear which has been implanted and only in  
25 special circumstances would this practice be altered.

The present invention therefore aims to provide a cochlear implant system which is capable of allowing more functionality to be incorporated in behind-the-ear units without increasing the sizes of such units and compromising the benefits which such systems provide to implant recipients.

30 Any discussion of documents, acts, materials, devices, articles or the like which has been included in the present specification is solely for the purpose of providing a context for the present invention. It is not to be taken as an admission that any or all of these matters form part of the prior art base or were common general knowledge in the field relevant to the present  
35 invention as it existed in Australia before the priority date of each claim of this application.

### Summary of the Invention

Throughout this specification the word "comprise", or variations such as "comprises" or "comprising", will be understood to imply the inclusion of a stated element, integer or step, or group of elements, integers or steps, but not  
5 the exclusion of any other element, integer or step, or group of elements, integers or steps.

As described, it is considered that with the increasing popularity of behind-the-ear units or even take up of in-the-ear units, cochlear implant system recipients will expect such devices to provide features additional to  
10 those considered as standard at present. The present invention is directed to meeting this expectation while ensuring that the unit remain at an acceptably small size. The additional features envisaged as being required as standard include: a built in telecoil for picking up signals from a telephone; the ability to detect sounds from both side of the head rather than just the side of the  
15 head that the BTE unit is positioned on; sufficient power resources to use all speech processing strategies; adequate battery life to enable the device to operate for a significant time without the need to recharge or replace the batteries; and a radio receiver and the like for classroom or other remote signal source use.

20 According to one aspect, the present application is directed to a first invention comprising a cochlear implant system comprising:

a first unit adapted to be worn on or in one ear of an implantee, the first unit having a case housing componentry including a microphone that detects sounds and outputs acoustic data signals representative of the detected  
25 sounds, and a speech processor means that receives the acoustic data signals;

a second unit adapted to be worn on or in the other ear of the implantee, the second unit having a case housing a power source; and

a power transmission means for transmitting power from the power source of the second unit to at least some of the componentry of the first unit.

30 The use of a power source in the second unit can provide a number of advantages. For example, the power source of the second unit can provide the implantee with more power or power for a longer time than is available from the use alone of an on-board power source. Saying this, the first unit can, in one embodiment, have an on-board power source.

35 The use of the power source in the second unit also potentially allows a reduction in the dimensions of the first unit as a smaller on-board power

source can potentially be utilised due to the presence of the additional power source in the second unit.

The speech processor means of the first unit can convert the received acoustic data signals into coded signals that are transmittable through a  
5 communication link to an implantable cochlear stimulator. The communication link preferably comprises a radio frequency link created between an external antenna coil and an implantable antenna coil. Other suitable communication links can be envisaged.

In this aspect, the second unit can further house a second microphone  
10 that detects sounds and outputs acoustic data signals representative of the detected sounds.

The power transmission means can comprise an electrical conduction means, such as electrically conducting wire or wires.

Still further, the system can comprise a signal transmission means  
15 whereby the acoustic data signals output by the second microphone are transmittable to the speech processor means of the first unit.

Where both are present, the signal transmission means and power transmission means can be housed in a common cable extending between the first unit and the second unit. It will, however, be appreciated that the  
20 respective signal transmission and power transmission means could comprise separate cables. Such one or more cables are preferably removably connectable with the first unit and/or the second unit. The one or more cables are preferably sufficiently long to just reach between the first and second unit, when such units are mounted on or in the respective ears of the  
25 implantee. In one embodiment, the one or more cables can be extendible or adjustable in length.

In another embodiment, the signal transmission means can comprise a wireless means, such as a short-distance radio frequency (RF) link.

In a further embodiment, the respective cases of the first unit and  
30 second unit can each have an ear hook extending therefrom to allow the cases to be worn behind the respective ears of the implantee. Instead, either or both of the first and second units can have a case adapted to be worn or fit within the ear canals of the implantee. In one embodiment, the case of the first unit is adapted to fit into one ear canal and the case of the second unit is  
35 adapted to fit into the ear canal of the other ear.

The second unit of the system can further house a receiver unit that detects signals from an external source and outputs acoustic data signals representative of the detected signals to the speech processor using the signal transmission means. The receiver unit can be selected from the group  
5 comprising a telecoil and a radio receiver.

In a further embodiment, the power source of the second unit can comprise one or more batteries. These batteries can be rechargeable.

In a preferred embodiment of this aspect, the power source of the second unit also provides power to at least some and preferably all of the  
10 componentry of the second unit. In another embodiment, the power source of the second unit can be used to provide power to all of the componentry of the first unit.

In a still further embodiment, the second unit has a switch means that, when operated can activate and deactivate componentry of the second unit.

15 In another embodiment, the second unit can house a second microphone that detects sounds and outputs acoustic data signals representative of the detected sounds, and a second speech processor means that receives the acoustic data signals and converts the signals into coded signals representative of the detected sounds, with the system further  
20 comprising a signal transmission means whereby the coded signals output by the second speech processor means are transmittable to the first unit.

In this embodiment, the second speech processor means can use a different speech processing strategy to that of the speech processor means housed in the first unit. In another embodiment, the second speech processor  
25 means can use the same speech processing strategy to that of the speech processor means housed in the first unit.

In this aspect, the first speech processor means of the first unit can be deactivated when the second speech processor means is in use. Such deactivation can occur automatically on commencement of use of the second  
30 unit or can be manually controlled by the implantee.

Where the first unit has an on-board power source, use of the power source of the second unit by the first unit can occur automatically on commencement of use of the second unit. For example, the first unit can be adapted to preferentially, and when available, draw power from the power  
35 source of the second unit on electrical connection of the second unit to the



first unit. In another embodiment, selection of which power source is utilised can be controlled by the implantee, a clinician or another person.

In another aspect, the present application is directed to a second invention comprising a cochlear implant system that in turn is comprised of:

5 a first unit adapted to be worn on or in one ear of an implantee, the first unit having a case housing componentry including a microphone that detects sounds and outputs acoustic data signals representative of the detected sounds, and a first speech processor means that receives the acoustic data signals;

10 a second unit adapted to be worn on or in the other ear of the implantee, the second unit having a case housing a power source, a second microphone that detects sounds and outputs acoustic data signals representative of the detected sounds, and a second speech processor means that receives the acoustic data signals and converts the signals into coded  
15 signals representative of the detected sounds;

a signal transmission means whereby the coded signals output by the second speech processor means are transmitted to the first unit; and

a power transmission means for transmitting power from the power source of the second unit to at least some of the componentry of the first unit.

20 In this aspect, the speech processor means of the first unit converts the received acoustic data signals of the first microphone and/or the coded signals of the second microphone and/or the second speech processor means into signals that are transmittable through a communication link to an implantable cochlear stimulator. In another embodiment, the second speech  
25 processor of the second unit can be adapted to convert received acoustic data signals from the second microphone and/or the first microphone and/or the first speech processor means. Transmission of the signals from the first microphone and/or the first speech processor means to the second speech processor means can be by the signal transmission means.

30 The communication link of this aspect preferably comprises a radio frequency link created between an external antenna coil and an implantable antenna coil. Other suitable communication links can be envisaged.

In this aspect, the speech processor means of the first unit can be deactivated when the second speech processor means is in use. Such  
35 deactivation can occur automatically on commencement of use of the second unit or can be manually controlled by the implantee. Still further, the second

speech processor means of the second unit can be deactivated when the first speech processor means is in use. Again, such deactivation can occur automatically on commencement of use of the first speech processor means.

In this aspect, the power transmission means can comprise an  
5 electrical conduction means, such as electrically conducting wire or wires. The signal transmission means and electrical conduction means can also be housed in a common cable extending between the first unit and the second unit. It will, however, be appreciated that the respective signal transmission means and electrical conduction means could comprise separate cables.  
10 Such one or more cables are preferably removably connectable with the first unit and/or second unit. Again, the one or more cables are preferably sufficiently long to just reach between the first and second unit, when such units are mounted on or in the respective ears of the implantee. In one embodiment, the one or more cables can be extendible or adjustable in  
15 length.

In another embodiment of this aspect, the signal transmission means can comprise a wireless means. For example, the wireless means can comprise a relatively short-distance radio frequency (RF) link.

In a further embodiment of this aspect, the respective cases of the first  
20 unit and second unit each have an ear hook extending therefrom to allow the cases to be worn behind the respective ears of the implantee. Instead, either or both of the first and second units can have a case adapted to be worn or fit within the ear canals of the implantee. In one embodiment, the case of the first unit is adapted to fit into one ear canal and the case of the second unit is  
25 adapted to fit into the ear canal of the other ear.

In a still further embodiment, the second unit further houses a receiver unit that detects signals from an external source and outputs acoustic data signals representative of the detected signals to the second speech processor means within the second unit and/or the first signal processor means housed  
30 within the first unit. Where the acoustic data signals are output to the speech processor means within the first unit, the signals are preferably transmittable using the signal transmission means as defined above. The receiver unit can be selected from the group comprising a telecoil and a radio receiver.

In a preferred embodiment of this aspect, the power source of the  
35 second unit can comprise one or more batteries. Said one or more batteries can be rechargeable batteries.

In a preferred embodiment of this aspect, the power source of the second unit provides power to at least some and preferably all of the componentry of the second unit. In another embodiment, the power source of the second unit can be used to provide power to all of the componentry of the first unit.

In a further embodiment, the first unit can have an-board power source.

In this aspect, where the first unit has an on-board power source, use of the power source of the second unit by the first unit can occur automatically on commencement of use of the second unit. For example, the first unit can be adapted to preferentially, and when available, draw power from the power source of the second unit on electrical connection of the second unit to the first unit. In another embodiment, selection of which power source is utilised can be controlled by the implantee, a clinician or another person.

In yet a further embodiment of this aspect, the second unit has a switch means that activates and deactivates componentry of the second unit.

In a still further embodiment, the first unit can be useable with an implantable unit. Such an implantable unit can be adapted to work, when necessary, in conjunction with the first unit. The implantable unit can though be adapted to work in a stand-alone mode.

The implantable unit can comprise:

(i) a hermetically sealed housing comprising:

- (a) an implantable power source that provides the power requirements of the implantable unit when operating in a stand-alone mode;
  - (b) an implantable microphone that detects sounds and outputs acoustic data signals representative of said detected sounds; and
  - (c) an implantable speech processor means that receives the acoustic data signals of the implantable microphone and converts the signals into stimulation signals representative of the detected sounds;
- (ii) an electrode array suitable for insertion in the cochlea of an implantee, the array once inserted being adapted to receive the stimulation signals from the implantable speech processor and output electrical stimulation to the implantee's auditory nerve; and

(iii) an antenna coil suitable for implantation in the implantee.

In this embodiment, an external antenna coil is inductively couplable with the antenna coil of the implantable unit to provide a radio frequency

(RF) link between the implantable cochlear stimulator and the first unit. This radio frequency link allows a coded signal output by the first speech processor housed within the first unit, and/or the second speech processor housed within the second unit, to be transmitted to the electrode array of the implantable unit. This may be desirable, for example, in instances where one or more components of the implantable unit are inoperable for any reason.

According to a still further aspect, the present application is directed to another invention comprising an accessory for use with a cochlear implant system, the system having an external component including a microphone that detects sounds and outputs acoustic data signals representative of the detected sounds, and a speech processor means that receives the acoustic data signals;

the accessory comprising:

a power source and power transmission means adapted to provide power to at least the external component of the cochlear implant system; and a second microphone that detects sounds and outputs acoustic data signals representative of the detected sounds to the speech processor means of the system.

The second microphone of this and the other aspects provided herein can be identical to the microphone used in the external component or first unit of the cochlear implant system. Where used, the second microphone can be used to provide binaural hearing for the implantee. The second microphone can be an electret-type microphone. In another embodiment, the second microphone can utilise a piezoelectric polymer or piezo-ceramic material.

The second microphone can comprise a hearing aid microphone as known in the art. An example of a suitable microphone is a Knowles microphone.

In the aspects, an electrically conducting lead can be used as a means of transmitting the acoustic data signals output from the second microphone of each of the aspects to the external component or first unit of the cochlear implant system. In another embodiment, the acoustic data signals can be transmitted by a wireless means. In one embodiment, the acoustic data signals can be transmitted by a relatively short-distance radio frequency (RF) link.

In this aspect, the accessory can further comprises a receiver unit that is adapted to detect signals from an external source, when present, and output acoustic data signals representative of the detected sounds to the speech processor means of the system.

5 In the aspects provided herein, the receiver unit can comprise a telecoil. Telecoils are used by hearing impaired listeners in particular situations which usually involve group situations in organised venues, such as classrooms, meeting halls, conference rooms, music halls, cinemas and the like. Telecoils are designed to pick up magnetic fields generated by wire  
10 loops which enclose the area. Telecoils are also used to pick up magnetic signals from a telephone to avoid acoustic interference in noisy situations.

In the aspects, the receiver unit can be adapted to receive frequency modulated (FM) and/or amplitude modulated (AM) signals. The receiver unit preferably includes a tuner means that allows an implantee or another person  
15 to tune the radio receiver to a desired FM or AM wavelength.

In the aspects, the power source of the accessory can comprise one or more batteries. The batteries can be rechargeable. The power source of the accessory preferably also provides power for the components of the accessory, such as the microphone. In another embodiment, the power  
20 source of the accessory can be used to provide a charging current to a rechargeable battery, if present, being used as an on-board power source for the external component or first unit of the cochlear implant system.

As previously described, the power transmission means can comprise an electrical conduction means, such as electrically conducting wire or wires  
25 that is preferably provided between the power source of the accessory and the external component or first unit of the cochlear implant system. The electrical connection can be provided by an electrically conducting lead that extends from the accessory or second unit to the external component or first unit of the cochlear implant system. The electrically conducting lead can be  
30 removably connectable to the external component and/or the accessory. The respective ends of the lead are preferably each removably insertable within sockets within both the accessory or second unit and the external component or first unit.

According to yet a further aspect, the present application is directed to  
35 another invention comprising an accessory for use with a cochlear implant

system, the implant having an external component including a microphone, and a speech processor means;

the accessory comprising:

a power source adapted to provide power to the external component of  
5 the cochlear implant system;

a second microphone that detects sounds and outputs acoustic data signals representative of the detected sounds to the speech processor; and

a receiver unit that detects signals from an external source, when present, and outputs acoustic data signals representative of the detected  
10 signals to the speech processor means of the system.

In a preferred embodiment of this aspect, the power source of the accessory, the microphone and the receiver unit of the accessory can have the features of the power source of the accessory, second microphone and receiver unit as defined above.

15 In this aspect, the cochlear implants system can have an on-board power source.

In this aspect, and where the first unit has an on-board power source, use of the power source of the accessory by the cochlear implant system can occur automatically on commencement of use of the accessory. For example,  
20 the cochlear implant system can be adapted to preferentially, and when available, draw power from the power source of the accessory on electrical connection of the accessory unit to the external component of the system. In another embodiment, selection of which power source is utilised can be controlled by the implantee, a clinician or another person.

25 In this aspect, the accessory can comprise a case that can be worn on the body, for example in a pouch or pocket. In a preferred embodiment, however, the case of the accessory is adapted to be worn behind the ear of the implantee that does not use the cochlear implant system. In another embodiment, the case of the accessory can be adapted to be worn within the  
30 ear canal of the ear of the implantee that does not use the cochlear implant system.

In a preferred embodiment, the accessory can include a switch means that activates and deactivates the accessory. The switch means can, for example, deactivate the accessory by disconnecting the power source from  
35 the circuitry for the other components of the accessory.

In another embodiment, the accessory can include a switch means that allows the implantee or another person to control which component of the accessory is in operation. For example, as the accessory includes both a microphone and a receiver unit, the switch means can be adapted to only  
5 allow one or the other of these components to operate at any particular time.

In a preferred embodiment of this aspect, the speech processor means of the implant receives the acoustic data signals and converts the signals into coded signals representative of the detected sounds.

In another embodiment of this aspect, the accessory can further  
10 comprise a second speech processor means that receives the acoustic data signals of the second microphone and converts the data signals into coded signals representative of the detected sounds. These coded signals can then be transmitted by the signal transmission means to the external component of the implant instead of, or in addition to, the acoustic data signals of the  
15 second microphone. The second speech processor can also be used to provide the implantee with the option of using sound coding algorithms not supported by the on-board speech processor within the external component of the cochlear implant system.

According to a still further aspect, the present application is directed to  
20 a still further invention comprising an accessory for use with a cochlear implant system, the cochlear implant system comprising an external component and an implantable component;

the external component including

a microphone that detects sounds and outputs acoustic data  
25 signals representative of the detected sounds;

an on-board power source; and

an external antenna coil;

the implantable component including

a cochlear stimulator; and  
30

an implantable antenna coil inductively couplable with the  
external coil to provide a radio frequency link between the external and  
internal component;

the accessory comprising:

a speech processor means that receives and processes the acoustic data  
35 signals of the microphone and converts the signals into coded signals that are transmittable from the accessory to the external component through a signal

transmission means and from the external component to the implantable cochlear stimulator through the radio frequency link.

In this aspect, the signal transmission means preferably provides a means of transmission of the acoustic data signals of the microphone to the  
5 speech processor means.

In one embodiment, the signal transmission means can be a wireless means.

In a still further embodiment of this aspect, the accessory can have a power source. In this case, an electrical conduction means can extend  
10 between the external component and the accessory to allow transmission of power from the on-board power source of the external component to at least the speech processor means of the accessory.

In a further embodiment, the accessory can further comprise a second microphone that detects sounds and also outputs acoustic data signals  
15 representative of the detected sounds to the speech processor means within the accessory.

In this aspect, the external component and/or accessory have a case, the respective cases of the external component and accessory each having an ear hook extending therefrom to allow the respective cases to be worn behind  
20 the respective ears of the implantee. The accessory can have a case adapted to be worn in an ear canal of an implantee. Still further, the external component can have a case adapted to be worn in an ear canal of an implantee. Yet further, the accessory and the external component each have a respective case adapted to worn in the respective ear canals of an  
25 implantee.

The accessory can further comprise a receiver unit that is adapted to detect signals from an external source, when present, and output acoustic data signals representative of the detected signals to the speech processor means. The receiver unit is preferably selected from the group comprising a  
30 telecoil and a radio receiver.

In all aspects, the cochlear implant system can include an implanted stimulator/receiver unit. The stimulator/receiver unit can include an electrode array adapted to be inserted into the cochlea.

The electrode array can be any type as is known in the art. It should be  
35 appreciated that the type of array used is not crucial to an understanding of



the present invention and any type of array can be used with the system of the present invention provided that it is supported by the system.

The implant system can also include one or more extracochlear electrodes to support monopolar stimulation.

5       The accessory or second unit can incorporate a warning system that provides an indication to the implantee or another person that the battery or batteries of the power source within the accessory needs replacing or recharging. The warning system may generate a unique stimulus signal that the implantee is trained to recognise as an indication that the battery or  
10 batteries needs replacing or recharging.

In another embodiment, the accessory or second unit can incorporate an interrogation means that allows the implantee or another person to determine the charge level of the battery or batteries in the accessory or second unit.

15       The inventions described herein provide an alternative means that allows the overall dimensions of the external component of a cochlear implant system to either remain substantially the same or be further reduced compared to presently known external components while offering improved performance and/or additional capabilities. It also provides the possibility of  
20 allowing for the operation of the cochlear implant system to be shared between the external components allowing the external components to be smaller in dimension and less visible. The present invention also provides the option of allowing the external components to be customised to the requirements of the implantee, taking into consideration the implantee's  
25 needs and preferences.

In a preferred embodiment of all aspects, the implanted component of the cochlear implant system includes a wire antenna coil. The antenna coil is preferably comprised of at least two, turns of electrically insulated wire tuned to parallel resonance by a capacitor. The electrical insulation of the antenna  
30 coil can be provided by a flexible silicone moulding and/or silicone or polyurethane tubing. The antenna coil is disposed about a centrally located magnet. The magnet can comprise a rare earth permanent magnet hermetically sealed within a titanium case. The magnet within its case is preferably held in the centre of the antenna coil by the silicone moulding  
35 surrounding the antenna coil. In a preferred embodiment, the magnet is removable from the system so as to allow the implantee to undergo magnetic

resonance imaging (MRI) scanning. Electrical connection between the coil and the other componentry of the implanted component can be provided by two hermetic and insulated ceramic feedthroughs or an electrical connector. The ceramic feedthroughs can be formed using the method described in  
5 abovementioned US Patent 5046242. The coil can act as a radio frequency (RF) link to allow bidirectional data transfer between the implanted component of the system and the external component.

The speech processor means of the cochlear implant system preferably performs an audio spectral analysis of the acoustic data signals and outputs  
10 channel amplitude levels. The speech processor means can also sort the outputs in order of magnitude or flag the spectral maxima as used in the SPEAK strategy developed by Cochlear Ltd.

The implanted component can include at least a stimulation processor that performs a stimulation strategy process, stimulus level mapping and  
15 output control. The input to the stimulation processor comes from the speech processor means, whether it be an implanted speech processor means or a speech processor means housed in an external component as defined herein. The role of the stimulation processor is well known in the art and has been performed in all conventional cochlear implant systems to deliver the  
20 stimulus to the intracochlea arrays. As such it is considered that a person skilled in the art would understand and appreciate the function performed by the stimulation processor in the current invention.

In another embodiment, the accessory or second unit as described above can include an external controller for the accessory, second unit and/or  
25 the cochlear implant system. Such a controller can provide a remote means of diagnosing and adjusting implant system parameters and also provide a means of selecting different speech processing strategies. For example, the controller can allow the implantee or a clinician to diagnose and adjust the sensitivity of the one or more speech processor means and/or the level of  
30 stimulation output by the electrode array.

The external controller also preferably provides the clinician or implantee with a means of interrogating the cochlear implant system to determine the status of the on-board power source, such as the level of charge of the battery, as well as other useful system information. The external  
35 controller also provides the clinician or implantee with a means of measuring the performance of the processor means and/or the microphone of the

cochlear implant system. The external controller can communicate with the cochlear implant system through an electrical lead or wireless radio frequency (RF) link between the accessory or second unit and the cochlear implant system.

5

#### Brief Description of the Drawings

By way of example only, embodiments of the present inventions are now described with reference to the accompanying drawings, in which:

Fig. 1 is a pictorial representation of a prior art cochlear implant  
10 system;

Fig. 2 is a schematic view of one embodiment of an accessory for a cochlear implant system according to the present invention; and

Fig. 3 is a pictorial representation of a cochlear implant system according to the present invention.

15

#### Preferred Mode of Carrying out the Invention

Before describing the features of the present invention, it is appropriate to briefly describe the construction of one type of known cochlear implant system with reference to Fig. 1.

20 One type of known cochlear implant system 5 typically consists of two main components, an external component including a speech processor 29, and an internal component including an implanted receiver and stimulator unit 22. The external component includes an on-board microphone 27. The speech processor 29 is, in this illustration, constructed and arranged so that it  
25 can fit behind the outer ear 11. Alternative versions may be worn on the body or within the ear canal 100. Attached to the speech processor 29 is a transmitter coil 24 which transmits electrical signals to the implanted unit 22 via a radio frequency (RF) link.

The implanted component includes a receiver coil 23 for receiving  
30 power and data from the transmitter coil 24. A cable 21 extends from the implanted receiver and stimulator unit 22 to the cochlea 12 and terminates in an electrode array 20. The signals thus received are applied by the array 20 to the basilar membrane 8 thereby stimulating the auditory nerve 9. The operation of such a device is described, for example, in US Patent No.  
35 4532930.

The speech processor 29 of the cochlear implant system 5 can perform an audio spectral analysis of the acoustic data signals from the microphone 27 and outputs channel amplitude levels. The speech processor 29 can also sort the outputs in order of magnitude or flag the spectral maxima as used in  
5 the SPEAK strategy developed by Cochlear Ltd.

One embodiment of an accessory for a cochlear implant system 5 according to the present invention is depicted schematically as 30 in Fig. 2. In this embodiment, the accessory 30 is adapted to be worn behind and supported by the ear of an implantee that is not implanted with the cochlear  
10 implant system 5. It will be appreciated that the accessory could also be supported in a pouch or pocket carried or worn by the implantee or adapted to be worn within the ear canal of the ear of the implantee that is not implanted with the cochlear implant system 5. The accessory 30 can be used in conjunction with the dedicated cochlear implant processor 29 as depicted  
15 in Fig. 1. The accessory 30 can, however, be used in conjunction with a totally implantable cochlear implant system having an implanted speech processor and microphone that is adapted to operate, at least for a certain period, in a stand-alone mode or an implant that is positioned within the ear canal 100 of the implantee. Still further, the accessory 30 can be adapted to  
20 be used with a speech processor 29 that is housed in a case that is adapted to be worn in the ear canal 100 of the implantee.

The accessory 30 has an external case 31 enclosing an additional power source 32. The power source 32 comprises one or more battery cells. The cells in the depicted embodiment are rechargeable.

25 The power source 32 can be used to provide power to the speech processor 29 and other componentry of the cochlear implant system 5 through electrical connection 33. The power provided by power source 32 can be used by the cochlear implant system 5 either in combination with or instead of any on-board power source within or electrically connected to the  
30 cochlear implant processor 29. The additional power source 32 can also be used to provide a charging current to a rechargeable battery being used as the on-board power source for the cochlear implant system 5. In another arrangement, the accessory 30 can be used with a cochlear implant system that does not have its own on-board power source. In this case, power for the  
35 cochlear implant system and the accessory 30 is provided by power source 32.

As depicted in Fig. 2, the accessory 30 can also include an additional microphone 34 and microphone signal amplifier 35. The microphone 34 detects sounds and outputs acoustic data signals representative of the detected sounds through the amplifier 35 to the speech processor 29 through  
5 signal connection 36.

In one embodiment, the additional microphone 34 can be identical to the microphone 27 used with the dedicated cochlear implant processor 29. When used, the additional microphone 34 provides binaural hearing for the implantee. The depicted additional microphone 34 is an electret-type  
10 microphone. In another embodiment, the additional microphone can utilise a piezoelectric polymer or piezo-ceramic material.

In the depicted embodiment, it is envisaged that signal connection 36 is provided by a cable extending between the case 31 of the accessory 30 and the cochlear implant processor 29. In another embodiment, the means of  
15 transmitting the acoustic data signals output from the additional microphone 34 to the cochlear implant processor 29 can comprise a wireless means. For example, the acoustic data signals could be transmitted by a relatively short-distance radio frequency (RF) link.

The depicted accessory 30 further includes an antenna 37 and radio  
20 receiver 38. The antenna 37 and receiver 38 detect radio frequency (RF) signals and output acoustic data signals representative of the detected radio frequency signals through signal connection 39 to the speech processor 29 of the cochlear implant system 5.

The accessory 30 can further comprise a telecoil system 40. Telecoils  
25 are used by implantees in situations such as classrooms, meeting halls, conference rooms, music halls and the like and pick up magnetic fields generated by wire loops which enclose the area. Telecoils are also used to pick up magnetic signals from a telephone to avoid acoustic interference in noisy situations. The telecoil 40 detects such signals and outputs signals  
30 representative of the detected signals to the speech processor 29 via signal connection 41

The receiver 38 can be tuned or switched to receive radio frequency signals of different frequencies. The receiver 38 can also be switched or tuned to receive frequency modulated (FM) and/or amplitude modulated  
35 (AM) signals. The radio receiver preferably includes a tuner means that

allows an implantee to tune the radio receiver to a desired FM or AM wavelength.

The additional power source 32 is also used in the accessory 30 to provide power for the components of the accessory, including the  
5 microphone 34, amplifier 35, receiver 38 and telecoil 40.

The accessory 30 can be provided with a switch that activates and deactivates the accessory 30. The switch can deactivate the accessory 30 by disconnecting the power source 32 from the circuitry for the other components, such as the amplifier 35, receiver 38 and telecoil 40.

10 The accessory 30 can also include a switch that allows the implantee to control which component of the accessory 30 is in operation. For example, where the accessory includes both the microphone 34 and the radio frequency receiver 38, the switch can be adapted to only allow one or the other of these components to operate at any particular time.

15 The accessory 30 can also incorporate a warning system that provides an indication to the implantee that the battery or batteries of the additional power source 32 needs replacing or recharging. The warning system may lead to the generation of a unique stimulus signal that the implantee is trained to recognise as an indication that the battery or batteries needs  
20 replacing or recharging.

In another embodiment, the accessory 30 can incorporate an interrogation means that allows the implantee to determine the charge level of the battery or batteries in the accessory 30.

In another embodiment, the accessory 30 can include an external  
25 controller for the accessory 30 and/or the dedicated cochlear implant processor 29. Such a controller can provide a remote means of diagnosing and adjusting implant or accessory parameters and also provide a means of selecting different speech processing strategies. For example, the controller can allow the implantee or a clinician to diagnose and adjust the sensitivity of  
30 the speech processor 29 and/or the level of stimulation output by the electrode array 20.

The external controller also preferably provides the clinician or implantee with a means of interrogating the cochlear implant system 5 or accessory 30 to determine the status of the on-board power source, such as  
35 the level of charge of the battery, as well as other useful system information. The external controller also provides the clinician or implantee with a means

of measuring the performance of the speech processor 29 and/or the microphone 27 of the cochlear implant processor 29. The external controller can communicate with the cochlear implant system 5 through an electrical lead or wireless RF link between the accessory 30 and the cochlear implant processor 29.

In another embodiment, and as depicted, the accessory 30 can include an on-board speech processor 50. The on-board speech processor 50 can also be used to provide the implantee with the option of using sound coding algorithms not supported by the speech processor 29 within the cochlear implant system 5. In the depicted embodiment, it is envisaged that a signal connection 51 between the speech processor 50 and the cochlear implant processor 29 is provided by a cable extending between the case 31 of the accessory 30 and the cochlear implant processor 29. In another embodiment, the means of transmitting the acoustic data signals output from the speech processor 50 to the cochlear implant processor 29 can comprise a wireless means. For example, the signals could be transmitted by a relatively short-distance radio frequency (RF) link.

It is envisaged that the accessory 30 of the present invention can incorporate any one or a number of elements 32, 34, 35, 37, 38, 40 and 50 as depicted in Figure 2, and remain within the scope of the present invention. For example, the accessory 30 may only comprise the speech processor 50. In this case, the speech processor 50 may receive acoustic data signals from the microphone 27, and/or a microphone 34 positioned on the accessory 30, and/or a microphone in another location. In this case, the cochlear implant system being used in conjunction with the accessory 30 may or may not have an on-board speech processor.

In the depicted embodiment, the electrical connections 33, 36, 39, 41 and 51 can be provided through a single cable that extends between the case of the speech processor 29 and the case 31 of the accessory 30. When the accessory 30 and speech processor 29 are being worn on the respective ears of the implantee, the cable can extend around the back of the head of the implantee.

Fig. 3 depicts one example of an accessory 30 being used in conjunction with the external component of a cochlear implant system 5. In this embodiment, both the external component of the cochlear implant system 5 and the accessory 30 have an ear hook 52. As depicted, the external

component of the cochlear implant system is adapted to be hooked to the right ear of the implantee and the accessory 30 is adapted to be hooked to the left ear of the implantee. It will, however, be appreciated that the respective locations of the cochlear implant processor 29 and accessory 30 could be readily swapped if in fact the implantee normally used the implant 5 with their left ear. While the respective cases of the cochlear implant processor 29 and the accessory 30 are depicted as having the same shape, it will be appreciated that the cases could be different shapes. The cochlear implant system 5 could also be different to that depicted, for example, the implant could be adapted to be worn in the ear canal of the implantee. Still further, the implant could be totally implantable cochlear implant system. Still further, the case of the accessory 30 could also be dimensioned and shaped to fit within the ear canal of the implantee.

In the embodiment depicted in Fig. 3, the cochlear implant system 5 has an on-board power source, a speech processor and a microphone 27. The accessory 30 also has a microphone 57, which in the depicted embodiment is identical to the microphone 27 mounted in the cochlear implant processor 29. Housed within the case 31 of the accessory 30 is a further power source. When the accessory 30 is used in conjunction with the cochlear implant system 5, the power source in the accessory can be used to provide power to componentry of the accessory 30 and the cochlear implant system 5. The transmission of power from the accessory 30 to the cochlear implant system 5 is provided by wiring housed within cable 58. Cable 58 is, in the depicted embodiment, removably connectable to the rear face of the respective components. The cable 58 can stretch to comfortably extend between the cochlear implant processor 29 and the accessory 30 when the respective components are mounted to the respective ears of the implantee. In normal use, it is envisaged that the cable 58 would extend around the back of the head of the implantee between the two ears.

It will be appreciated that the case 31 could house a speech processor or other componentry as has been described herein. Signal connection from the accessory 30 to the cochlear implant system 5 for this componentry can also be provided by appropriate wiring housed within cable 58. As already described, the speech processor in the accessory 30 can be used instead of or in conjunction with the speech processor housed in the cochlear implant system 5.



It will be appreciated by persons skilled in the art that numerous variations and/or modifications may be made to the invention as shown in the specific embodiments without departing from the spirit or scope of the invention as broadly described. The present embodiments are, therefore, to  
5 be considered in all respects as illustrative and not restrictive.

## CLAIMS:

1. A cochlear implant system comprising:  
a first unit adapted to be worn on or in one ear of an implantee, the first  
5 unit having a case housing componentry including a microphone that detects  
sounds and outputs acoustic data signals representative of the detected  
sounds, and a speech processor means that receives the acoustic data signals;  
a second unit adapted to be worn on or in the other ear of the  
implantee, the second unit having a case housing a power source; and  
10 a power transmission means for transmitting power from the power  
source of the second unit to at least some of the componentry of the first unit.
2. A cochlear implant system of claim 1 wherein the speech processor  
means converts the received acoustic data signals into coded signals that are  
15 transmittable through a communication link to an implantable cochlear  
stimulator.
3. A cochlear implant system of claim 2 wherein the second unit further  
houses a second microphone that detects sounds and outputs acoustic data  
20 signals representative of the detected sounds.
4. A cochlear implant system of claim 3 further comprising signal  
transmission means whereby the acoustic data signals output by the second  
microphone are transmittable to the speech processor means of the first unit.  
25
5. A cochlear implant system of claim 4 wherein the power transmission  
means comprises an electrical conduction means and the signal transmission  
means and electrical conduction means are housed in a common cable  
extending between the first unit and the second unit.  
30
6. A cochlear implant system of claim 4 wherein the signal transmission  
means comprises a wireless means.
7. A cochlear implant system of claim 6 wherein the wireless means  
35 comprises a short-distance radio frequency link.

8 A cochlear implant system of claim 1 wherein the respective cases of the first unit and second unit each have an ear hook extending therefrom to allow the respective cases to be worn behind the respective ears of the implantee.

5

9. A cochlear implant system of claim 4 wherein the second unit further houses a receiver unit that detects signals from an external source and outputs acoustic data signals representative of the detected signals to the speech processor means using the signal transmission means.

10

10. A cochlear implant system of claim 9 wherein the receiver unit is selected from the group comprising a telecoil and a radio receiver.

11. A cochlear implant system of claim 1 wherein the power source of the  
15 second unit comprises one or more batteries.

12. A cochlear implant system of claim 11 wherein said one or more batteries are rechargeable.

20 13. A cochlear implant system of claim 11 wherein the power source of the second unit also provides power to componentry of the second unit.

14. A cochlear implant system of claim 1 wherein the second unit has a switch means that activates and deactivates componentry of the second unit.

25

15. A cochlear implant system of claim 1 wherein the case of the second unit further houses a second microphone that detects sounds and outputs acoustic data signals representative of the detected sounds, and a second speech processor means that receives the acoustic data signals and converts  
30 the signals into coded signals representative of the detected sounds, the system further comprising a signal transmission means whereby the coded signals output by the second speech processor means are transmittable to the first unit.

16. A cochlear system of claim 15 wherein the second speech processor means uses a different speech processing strategy to that of the speech processor means housed within the first unit.

5 17. A cochlear implant system comprising:

a first unit adapted to be worn on or in one ear of an implantee, the first unit having a case housing componentry including a first microphone that detects sounds and outputs acoustic data signals representative of the detected sounds, and a first speech processor means that receives the acoustic  
10 data signals;

a second unit adapted to be worn on or in the other ear of the implantee, the second unit having a case housing a second power source, a second microphone that also detects sounds and outputs acoustic data signals representative of the detected sounds, and a second speech processor means  
15 that receives the acoustic data signals and converts the signals into coded signals representative of the detected sounds;

a signal transmission means whereby the coded signals output by the second speech processor means are transmittable to the first unit; and

a power transmission means for transmitting power from the power  
20 source to at least some of the componentry of the first unit.

18. A cochlear implant system of claim 17 wherein the speech processor means of the first unit converts the received acoustic data signals of the first microphone and/or the coded signals of the second speech processor means  
25 into signals that are transmittable through a communication link to an implantable cochlear stimulator.

19. A cochlear implant system of claim 18 wherein the power transmission means comprises an electrical conduction means and the signal transmission  
30 means and electrical conduction means are housed in a common cable extending between the first unit and the second unit.

20. A cochlear implant system of claim 18 wherein the signal transmission means comprises a wireless means.

21. A cochlear implant system of claim 20 wherein the wireless means comprises a relatively short-distance radio frequency link.
- 22 A cochlear implant system of claim 18 wherein the respective cases of  
5 the first unit and second unit each have an ear hook extending therefrom to allow the respective cases to be worn behind the respective ears of the implantee.
23. A cochlear implant system of claim 18 wherein the case of the second  
10 unit further houses a receiver unit that detects signals from an external source and outputs acoustic data signals representative of the detected signals to the second speech processor means within the second unit and/or the first signal processor means housed within the first unit.
- 15 24. A cochlear implant system of claim 23 wherein the receiver unit is selected from the group comprising a telecoil and a radio receiver.
25. A cochlear implant system of claim 18 wherein the power source of the  
20 second unit comprises one or more batteries.
26. A cochlear implant system of claim 25 wherein said one or more batteries are rechargeable.
27. A cochlear implant system of claim 25 wherein the power source  
25 provides power to componentry of the second unit.
28. A cochlear implant system of claim 18 wherein the second unit has a switch means that activates and deactivates componentry of the second unit.
- 30 29. A cochlear implant system of claim 18 wherein the first unit is useable with an implantable cochlear stimulator that is adapted to work in a stand-alone mode and, when necessary, in conjunction with the first unit, wherein:  
the implantable cochlear stimulator comprises:  
(i) a hermetically sealed housing comprising:  
35 (a) an implantable power source that provides the power requirements of the implantable unit when operating in a stand-alone mode;

(b) an implantable microphone that detects sounds and outputs acoustic data signals representative of said detected sounds; and

(c) an implantable speech processor means that receives said acoustic data signals of the implantable microphone and converts the signals  
5 into stimulation signals representative of the detected sounds;

(ii) an electrode array suitable for insertion in the cochlea of an implantee, the array once inserted being adapted to receive the stimulation signals from the implantable speech processor and output electrical stimulation to the implantee's auditory nerve; and

10 (iii) an antenna coil suitable for implantation in the implantee;  
wherein an external antenna coil is inductively couplable with the antenna coil of the implantable cochlear stimulator to provide a radio frequency link between the implantable cochlear stimulator and the first unit, and further wherein a coded signal output by the first speech processor  
15 means housed within the first unit and/or the second speech processor means housed within the second unit is transmittable to the electrode array through the radio frequency link.

30. An accessory for use with a cochlear implant system, the cochlear  
20 implant system comprising an external component including a microphone that detects sounds and outputs acoustic data signals representative of the detected sounds, and a speech processor means that receives the acoustic data signals;

the accessory comprising:

25 a power source and power transmission means adapted to provide power to at least the external component of the cochlear implant system; and

a second microphone that also detects sounds and outputs acoustic data signals representative of the detected sounds to the speech processor means of the system.

30 31. An accessory of claim 30 wherein the speech processor means converts the received acoustic data signals into coded signals that are transmittable through a communication link to an implantable cochlear stimulator.

32. An accessory of claim 30 wherein the power transmission means  
35 comprises an electrical conduction means, the electrical conduction means

being removably connectable between the external component and the accessory.

33. An accessory of claim 32 wherein the coded signals output by the  
5 second microphone are transmittable to the speech processor of the system by a signal transmission means.

34. An accessory of claim 33 wherein the signal transmission means and electrical conduction means are housed in a common cable extending  
10 between the external component and the accessory.

35. An accessory of claim 33 wherein the signal transmission means comprises a wireless means.

15 36. An accessory of claim 35 wherein the wireless means comprises a relatively short-distance radio frequency link.

37. An accessory of claim 31 wherein the implant and accessory each have a case, the respective cases of the implant and accessory each having an ear  
20 hook extending therefrom to allow the respective cases to be worn behind the respective ears of the implantee.

38. An accessory of claim 31 wherein the accessory further comprises a receiver unit, the receiver unit being selected from the group comprising a  
25 telecoil and a radio receiver.

39. An accessory of claim 31 wherein the power source of the accessory comprises one or more batteries.

30 40. An accessory of claim 39 wherein said one or more batteries are rechargeable.

41. An accessory of claim 31 wherein the power source of the accessory provides power to componentry of the accessory.

42. An accessory of claim 31 wherein the accessory has a switch means that activates and deactivates componentry of the accessory.

43. An accessory for use with a cochlear implant system, the cochlear  
5 implant system comprising an external component and an implantable component;  
the external component including  
a microphone that detects sounds and outputs acoustic data  
signals representative of the detected sounds;  
10 an on-board power source; and  
an external antenna coil;  
the implantable component including  
a cochlear stimulator; and  
an implantable antenna coil inductively couplable with the  
15 external coil to provide a radio frequency link between the external and internal component;  
the accessory comprising:  
a speech processor means that receives and processes the acoustic data signals of the microphone and converts the signals into coded signals that are  
20 transmittable from the accessory to the external component through a signal transmission means and from the external component to the implantable cochlear stimulator through the radio frequency link.

44. An accessory of claim 43 wherein the signal transmission means  
25 provides a means of transmission of the acoustic data signals of the microphone to the speech processor means.

45. An accessory of claim 43 or claim 44 wherein the signal transmission means is a wireless means.  
30

46. An accessory of any one of claims 43 to 45 wherein the accessory has a power source.

47. An accessory of any one of claims 43 to 45 wherein an electrical  
35 conduction means extends between the external component and the accessory to allow transmission of power from the on-board power source of



the external component to at least the speech processor means of the accessory.

48. An accessory of claim 43 wherein the accessory further comprises a  
5 second microphone that detects sounds and also outputs acoustic data signals representative of the detected sounds to the speech processor means within the accessory.

49. An accessory of any one of claims 43 to 48 wherein the external  
10 component and/or accessory have a case, the respective cases of the external component and accessory each having an ear hook extending therefrom to allow the respective cases to be worn behind the respective ears of the implantee.

15 50. An accessory of any one of claims 43 to 48 wherein the accessory has a case adapted to be worn in an ear canal of an implantee.

51. An accessory of any one of claims 43 to 48 wherein the external  
component has a case adapted to be worn in an ear canal of an implantee.  
20

52. An accessory of any one of claims 43 to 48 wherein the accessory and the external component each have a respective case adapted to worn in the respective ear canals of an implantee.

25 53. An accessory of any one of claims 43 to 52 wherein the accessory further comprises a receiver unit that is adapted to detect signals from an external source, when present, and output acoustic data signals representative of the detected signals to the speech processor means.

30 54. An accessory of claim 53 wherein the receiver unit is selected from the group comprising a telecoil and a radio receiver.

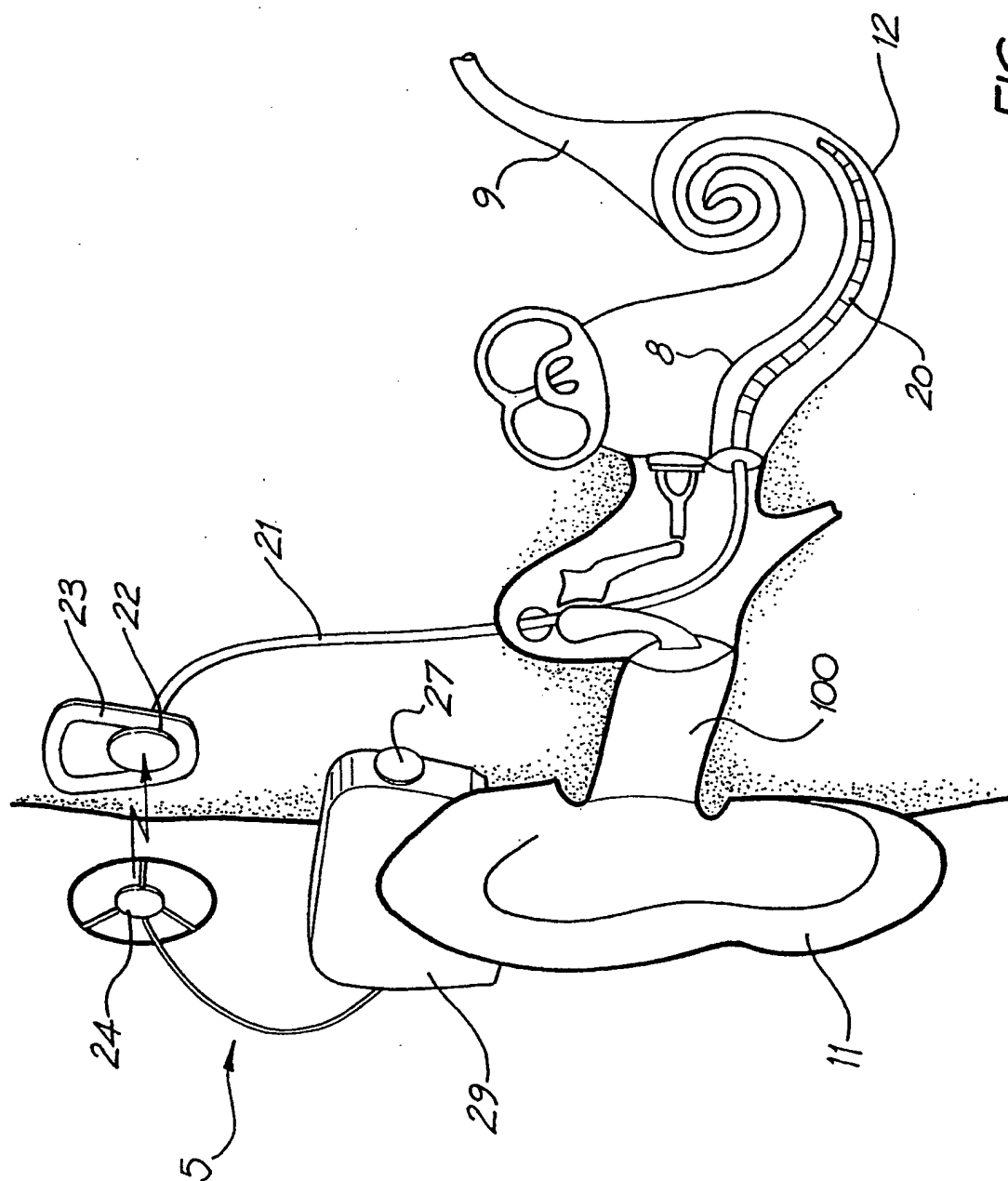


FIG. 1

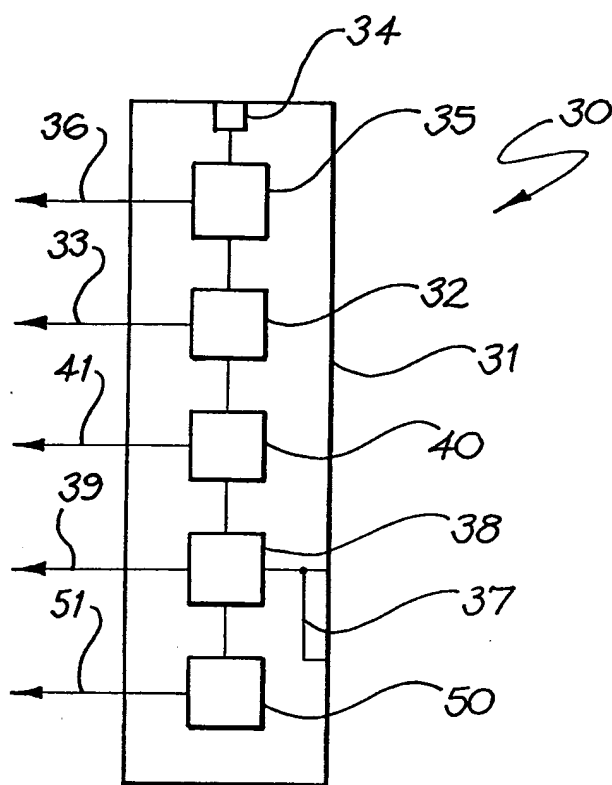
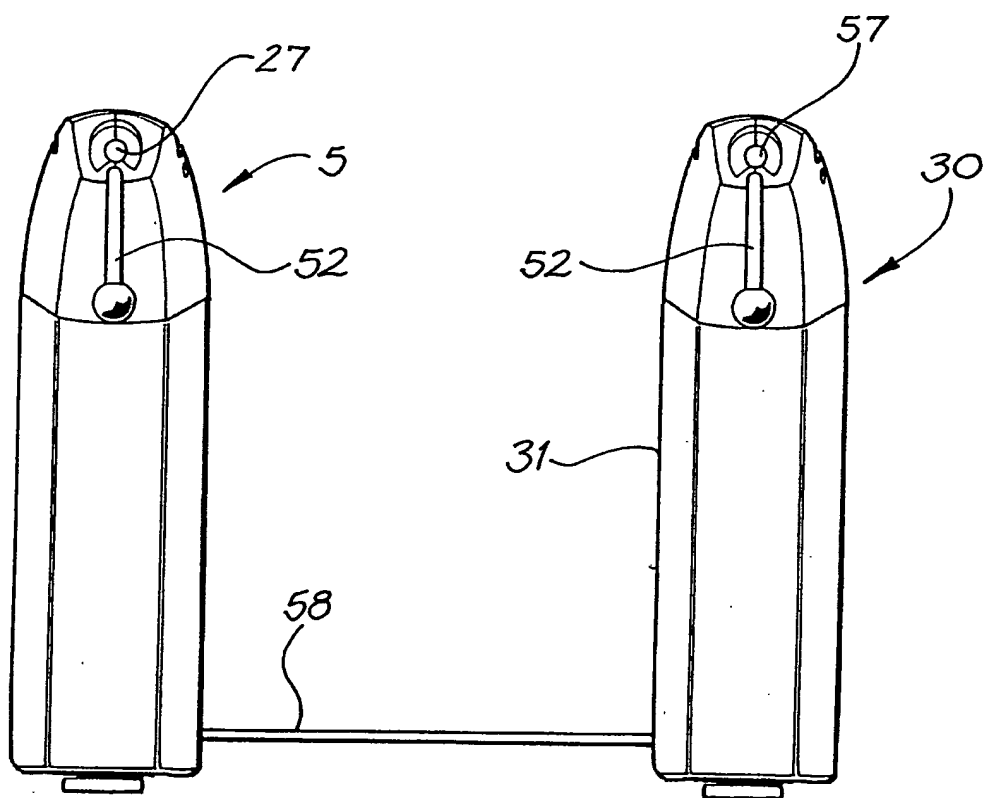


FIG. 2

*FIG. 3*

## INTERNATIONAL SEARCH REPORT

International application No.

PCT/AU02/00036

<b>A. CLASSIFICATION OF SUBJECT MATTER</b>		
Int. Cl. <sup>7</sup> : H04R 25/00, A61N 1/36		
According to International Patent Classification (IPC) or to both national classification and IPC		
<b>B. FIELDS SEARCHED</b>		
Minimum documentation searched (classification system followed by classification symbols)		
Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched		
Electronic data base consulted during the international search (name of data base and, where practicable, search terms used) WPAT, Internet: cochlear, implant, stimulator		
<b>C. DOCUMENTS CONSIDERED TO BE RELEVANT</b>		
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 5824022 A (ZILBERMAN et al) 20 October 1998 Column 2 line 50 to column 3 line 8, figure 5	43-54
<input type="checkbox"/> Further documents are listed in the continuation of Box C <input checked="" type="checkbox"/> See patent family annex		
<p>* Special categories of cited documents:</p> <p>"A" document defining the general state of the art which is not considered to be of particular relevance</p> <p>"E" earlier application or patent but published on or after the international filing date</p> <p>"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)</p> <p>"O" document referring to an oral disclosure, use, exhibition or other means</p> <p>"P" document published prior to the international filing date but later than the priority date claimed</p> <p>"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention</p> <p>"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone</p> <p>"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art</p> <p>"&amp;" document member of the same patent family</p>		
Date of the actual completion of the international search 13 February 2002		Date of mailing of the international search report 18 FEB 2002
Name and mailing address of the ISA/AU AUSTRALIAN PATENT OFFICE PO BOX 200, WODEN ACT 2606, AUSTRALIA E-mail address: pct@ipaustalia.gov.au Facsimile No. (02) 6285 3929		Authorized officer  DEREK BARNES Telephone No : (02) 6283 2198

**INTERNATIONAL SEARCH REPORT**  
Information on patent family members

International application No.  
**PCT/AU02/00036**

This Annex lists the known "A" publication level patent family members relating to the patent documents cited in the above-mentioned international search report. The Australian Patent Office is in no way liable for these particulars which are merely given for the purpose of information.

Patent Document Cited in Search Report		Patent Family Member
US	5824022	NONE
END OF ANNEX		